

## Research Article

# Formulation and Statistical Optimization of Pulsatile Drug Delivery System for Terbutaline Sulphate

Mohan Vikas<sup>1\*</sup>, Chandu Babu Rao<sup>2</sup>

<sup>1</sup>Department of Pharmaceutical Sciences, Acharya Nagarjuna University, India

<sup>2</sup>Department of Pharmaceutical, Pridarshini Institute of Pharmaceutical Sciences, India

\*Address Correspondence to Mohan Vikas, E-mail: mohanvikas@gmail.com

**Received:** 01 March 2023; Manuscript No: JDAR-23-96342; **Editor assigned:** 03 March 2023; PreQC No: JDAR-23-96342 (PQ); **Reviewed:** 17 March 2023; QC No: JDAR-23-96342; **Revised:** 22 March 2023; Manuscript No: JDAR-23-96342 (R); **Published:** 29 March 2023; **DOI:** 10.4303/JDAR/236230

Copyright © 2023 Mohan Vikas, et al. This is an open access article distributed under the terms of the Creative Commons Attribution License, which permits unrestricted use, distribution, and reproduction in any medium, provided the original work is properly cited.

### Abstract

In the present work it was aimed at developing chrono modulated drug delivery formulation for the treatment of nocturnal asthma. To determine the authenticity of the drug sample (Terbutaline sulphate), various physical, physicochemical and spectrophotometric methods were employed. UV and FTIR spectroscopy were used to verify the authenticity of the sample and the sample was found to be authentic. Drug polymer compatibility studies were conducted and no sign of physical compatibility was seen. The FTIR studies of physical mixture of the drug with different polymers showed no sign of interaction as the spectra of mixtures showed the peaks similar to pure drug spectra. UV spectroscopic method was selected as preferred analytical method for determination of terbutaline sulphate. Trial batches (preliminary) were formulated to study influence of polymer concentration on the physical properties and release profiles of the formulations. The final concentration of the polymers to be used in experimental design was fixed using the preliminary trial batches data.

**Keywords:** Terbutaline sulphate; Chrono modulated drug delivery; FTIR; DSC

### Introduction

The use of medicines in curing diseases started very early in history. The ancient texts found in China and Egypt mention many types of remedies out of which some are considered useful till date [1]. As the science of medicine developed, the concept of homeostasis was solely used to treat diseases. This theory states that the occurrence of symptoms of a disease and response to medication does not depend on the time, day or month. This concept of homeostasis is being challenged by recent research in this field. The research in this field has shown that most human functions are organized in time and repeat after regular time intervals ranging from hours to months [2].

### Chronobiology

Chronobiology is defined as the study of Biological Rhythms (BR) mechanisms behind them. From the ancient

time, relation between time and biological functions had been studied. Circadian means showing rhythmic behavior. Many biological functions such as nerve impulse, heart-beat, sleep and menstrual cycles show rhythmic behavior. The time between each repetition of such biological functions is called as a period. Usually, the Circadian Rhythms (CR) have a period of 20 h to 28 h between each repetition. BR in humans and animals has been documented by a large number of studies published in respected scientific journals [3-5].

### Mechanisms of biological time-keeping

Master Biological Clock, the Suprachiasmatic Nuclei (SCN)

### Mechanisms of biological time-keeping

Master clock which comprises of paired SCN present in the pineal and hypothalamus gland control the BR [6-9]. The time keeping system (responsible for rhythmic activities) is made of various genes and their gene products (Clock genes, Per1, Per2, Per3, B<sub>mal</sub>, Clock and Cry). The expression of clock genes (Cry1, Cry2, Per1, Per2) is done by transcription factors such as CLOCK and BMAL1. Circadian rhythm in the expression of the CLOCK: BMAL1 driven clock and clock-controlled genes is controlled by negative feedback of proteins PER and CRY. Rhythm stabilization is controlled by feedback loops, which include genes Rev-erba and Rora. The 24-hour night dark cycle also affects the precision of period of CR by modulation (post-translational) of clock proteins [10]. The peripheral circadian clocks which are located in other parts of body (cells, tissue and organs) are also controlled by master SCN. The output given by both the central and peripheral clocks is harmonized by clock-controlled genes leading to making of Circadian

Time Structure (CTS). The biological time-keeping system also includes the multitude of peripheral circadian clocks located in cells, tissues and organs, which are regulated by the master SCN clock [11]. The output of the central and peripheral circadian clocks is mediated by various clock-controlled genes, giving rise to the body's CTS.

### **Drug delivery systems for chronotherapeutic delivery of drugs**

Chronotherapy of nocturnal asthma requires either constant plasma drug concentration maintenance throughout the night for patients having attacks at any time during night or delivery of drug during morning hours for patients having asthma attacks only during morning hours. To meet such requirements both type of systems have been formulated. Pulsatile drug delivery systems release drug quickly after a time gap known as lag time to match the circadian rhythm of a disease [12]. Various external signals or stimuli can start the release of drug from pulsatile systems such as chemical, magnetic, thermal and electrical stimuli and also the start of release can be regulated by time period as in time-controlled devices.

#### **Advantages of pulsatile delivery**

- Reduced side effects.
- The daytime or night-time activity is extended.
- Dosing frequency is reduced.
- The dose size is reduced.
- More suitable for patients.
- As the numbers of doses are less, overall cost of treatment is reduced.
- Drug more suitably adapts to CR of diseases and body functions.
- Specific sites such as colon can be targeted.
- As some drugs can be released in colon the stomach mucosa is protected from drugs which irritate.
- As the drugs are released in colon the hepatic first pass is prevented increasing bioavailability.

#### **Various types of pulsatile drug delivery systems**

Formulations dependent on release-controlling coatings: In such formulations the solid core (active ingredient) is coated with polymers which can affect the time of the release of active ingredient. Single or multi-units can be formulated into the core. Multiple units have advantages as they offer consistent release due to low effect of gastric residence time. Depending upon the type of polymer used in coating the release of drug can be categorized into various mechanisms.

a) Erodible systems: In these systems core is coated with a hydrophilic polymeric coating of an adequate thickness which when exposed to gastric fluid, swells, dissolves or erodes. This leads to delay in the release of active ingredient from the formulation. The type of polymer, its coating

level and concentration effects the lag time. Hydrophilic polymers (cellulose derivatives), such as hydroxypropylcellulose, hydroxyethylcellulose, and hydroxypropylmethylcellulose and are mostly used due to versatile properties and established safety.

b) Rupturable systems: In these systems desired lag time is achieved by the liberation of the active pharmaceutical ingredient by the breaking of films, which are moderately permeable to water. These films are made of water insoluble polymers and sometime pore formers are also added. As the water enters into the core due to osmotic pressure the swellable polymer in the core swells leading to the rupturing of the film leading to release of active ingredient. The composition and thickness of the coating controls the time of drug release.

c) Diffusive reservoir systems: In these systems polymeric films with increasing permeability made of Eudragit® RS are applied to a core containing the active ingredient. These systems show sigmoidal release pattern due to the fact that initially the diffusion of water into the core is limited, which cause partial ionization of the organic acid present in the in between layer.

#### **Delivery systems based on release-controlling plugs**

In such systems an impermeable capsule shell body is sealed with a hydrophilic plug which when comes in contact with water swells leading to its expulsion. After the complete removal of plug the drug is released. The lag time is dependent upon the composition of plug material. Various erodible hydrophilic polymers, such as HPMC, PEO, sodium alginate, PVA and guar gum are used to make plug and the insoluble capsule shell is made of formaldehyde treated gelatin or ethyl cellulose.

#### **Delivery systems based on osmotic pumping**

In this system the core is made of 2 parts divided by a partition. One part contains active ingredient and other part contains expanding polymers. The core completely encapsulated in semi-permeable film coat. Holes are made in this shell-using laser. These holes connect the drug with the dissolution medium. The release can be further delayed by interposing a hydrophilic coat between the core and the outer membrane. When water enters into the core the drug dissolves and is pushed at a constant rate out by the swellable polymer through the laser-drilled hole.

#### **Materials**

Terbutaline sulphate, HPMC K15M, Avicel PH-101 were procured from Oscar Remedies Pvt. Ltd. Haryana, India. Ethyl cellulose, Ac-Di-Sol, Sodium starch glycolate, Avicel PH-101, Lactose, Talc were obtained from Nice Chemicals Pvt. Ltd. Kerala, India. All other ingredients were also analytical grade.

#### **Methods**

##### **Drug analysis**

Analysis of Terbutaline sulphate was done to identify the obtained sample. Organoleptic properties of the pure drug

were found out. Melting point, solubility and partition coefficient of the drug were determined.

### Determination of melting point

Capillary fusion method was used to determine the melting point of Terbutaline sulphate using Remi's melting point apparatus. Melting point was noted and verified from literature value.

### Determination of absorption maxima ( $\lambda_{\max}$ ) for analysis

Solution of Terbutaline sulphate was prepared in the buffer pH 1.2.  $\lambda_{\max}$  was determined by scanning between 200 nm-400 nm, using UV spectrophotometer. The scanned  $\lambda_{\max}$  values were compared with literature value (Clarkes Analysis of drugs and poisons).

### Fourier transform infrared analysis

The FTIR analysis is used to compare drug sample with a pure authentic sample. The data is used to verify the purity of the sample drug. 3 mg-5 mg of drug sample was taken and grinded with KBr and compacted into a pellet. The pellet was analyzed in the spectrophotometer in wavelength 4000  $\text{cm}^{-1}$  to 400  $\text{cm}^{-1}$ .

### Calibration curve

Calibration curve of Terbutaline sulphate in Hydrochloric acid buffer (pH 1.2) and phosphate buffer (pH 6.8). Calibration curve was plotted in a range of 2  $\mu\text{g/ml}$ -18  $\mu\text{g/ml}$ . Absorbance was determined using UV-Visible spectrophotometer at 276 nm.

### Solubility study

The solubility of Terbutaline sulphate was determined in water. A definite but excess quantity (1500 mg) of drug was dissolved in 5 ml of distilled water in 10 ml volumetric flasks. The drug was dissolved using a shaker water bath at Experimental design for formulating fast release tablet. The UV absorbance of the solution after appropriate dilutions was determined at 276 nm using UV spectrophotometer and the amount of drug dissolved was calculated using

calibration curve.

### Partition co-efficient

A major criterion in evaluation of the ability of a drug to penetrate the lipid membrane is its apparent oil/water partition coefficient ( $K_{o/w}$ ). The partition coefficient of Terbutaline sulphate was determined in n-octanol: Phosphate buffer pH 7.4. 10 mg of Terbutaline sulphate was added to 10 ml of n-octanol: Phosphate buffer pH 7.4 (1:1), in a separating funnel and shaken. Both the layers were separated and the analysis of the Terbutaline sulphate, which was solubilized in aqueous phase, was determined by measuring the absorbance at 276 nm using UV spectrophotometer. Partition coefficient of Terbutaline sulphate was calculated using equation (1). The partition coefficient value was calculated and compared with literature value.

$$P_{o/w} = (C_{\text{oil}}/C_{\text{water}}) \text{ equilibrium (1)}$$

### Drug polymer interaction studies

The drug polymer interaction was studied. Desired quantity of drug with specified excipients (HPMC 15M, Carbopol 971P, Ac-Di-Sol and Ethyl cellulose) were taken in the ratio 1:1 and 1:5 and mixed thoroughly and filled in dried vials. The vials were sealed and kept at 45°C for 2 weeks. The vials were examined daily at regular interval for discoloration, clump formulation and liquefaction. The FTIR analysis was done in a range between 400  $\text{cm}^{-1}$ -4000  $\text{cm}^{-1}$ . The obtained spectra were then studied for difference in the peaks obtained by comparing with the spectra of pure drug.

### Formulation of fast-release tablets

The direct compression technique was used for tablet preparation. All the raw materials were passed through a#60 (0.250 mm) sieve before mixing (Table 1). Terbutaline sulphate, sodium starch glycolate, Ac-Di-Sol, lactose and Avicel PH-101. The blending was done employing a laboratory mortar and pestle. The powder blend was lubricated with 2% talc and 2% magnesium stearate. The powder blend (100 mg) was compressed using a 6-mm tooling punch on a single punch tablet machine.

**Table 1:** Composition of preliminary trial batches of Terbutaline sulphate fast-release tablet formulation (Batches TF1-TF16 in %w/w)

Ingredients	TF1	TF2	TF3	TF4	TF5	TF6	TF7	TF8	TF9	TF10	TF11	TF12	TF13	TF14	TF15	TF16
Terbutaline Sulphate	2	2	2	2	2	2	2	2	2	2	2	2	2	2	2	2
Ac-Di-Sol	1	2	3	4	5	6	0	0	0	0	0	0	1	3	6	9
Sodium starch glycolate	0	0	0	0	0	0	1	2	3	4	5	6	1	3	6	9
Avicel PH -101	30	30	30	30	30	30	30	30	30	30	30	30	30	30	30	30
Lactose	63	62	61	60	59	58	63	62	61	60	59	58	62	58	52	46
Magnesium stearate	2	2	2	2	2	2	2	2	2	2	2	2	2	2	2	2
Talc	2	2	2	2	2	2	2	2	2	2	2	2	2	2	2	2

### Pre-compression characterization of FRT powder blends

The powder blends of FRT were evaluated for flow properties, which included Hausner's ratio, bulk density, com-

pressibility index, tapped density, and angle of repose. Study of these properties is essential as poor flow properties can cause problem of powder not flowing from hopper into the die, which makes it impossible to work on rotary tableting machines.

### Bulk density ( $\rho_b$ )

A weighed amount (M) of powder blend was added to a graduated measuring cylinder and its volume (Vb) was found.

### Compressibility index (I)

Compressibility index is an indication of flow properties of powder less is the value of co.

### Hausner's ratio (HR)

It indicates flow properties of powder blend. Lower value of Hausner's ratio (<1.25) is an indicator of better flow properties, compressibility index better is the flow and vice versa.

### Angle of repose ( $\theta$ )

Angle of Repose is also an indicative of flow properties, values of <25 means excellent flow properties and values of >40 are indicative of poor flow properties.

### Post-compression characterization

Formulated FRT were tested for characteristics like thickness, friability, hardness, drug content, disintegration time and *in vitro* release studies.

### General appearance

Tablets were evaluated for tablet's size, colour, shape, odour, surface texture, physical flaws.

### Tablet thickness

Thickness of 10 units (tablets) was measured using Vernier caliper.

### Weight variation

Tablets were evaluated for weight variation. As per USP, 20 tablets were taken and weighed separately, then their mean weight was determined, and the individual tablet weights were compared to the mean weight for weight variation.

### Hardness

Pfizer hardness tester was used to check hardness of the tablets.

### Friability

Tablets were evaluated for friability using Roche friabilator. In this test, the tablets are subjected to abrasions and shock.

### Drug content

FRT were evaluated for drug content. 10 tablets from each

formulation batch were weighed powdered. Then powder equivalent to 2 mg was dissolved in 0.1N HCl and drug content was determined spectrophotometrically at 276 nm.

### Disintegration time

USP-27/NF-22 disintegration test apparatus was used for this test and standard method was followed.

### Experimental design for formulating fast release tablet

A 3<sup>2</sup> design was used. In accordance to this design total nine experiments were done. This design consists of dependent variables Y and independent or controlled variables X<sub>1</sub> and X<sub>2</sub>. The 2 independent formulation variables selected for this study were X<sub>1</sub>, amount of Ac-Di-Sol; and X<sub>2</sub>, amount of Sodium starch glycolate. The independent variables were varied at 3 levels. The levels for these 3 parameters were determined from the preliminary trials. The dependent variables were Y<sub>1</sub> i.e., disintegration time in seconds; Y<sub>2</sub> i.e., friability in %weight. Tables 2 and 3 summarize the factors, the levels tested, and the actual values of the coded variables.

**Table 2:** Factors combinations as per the chosen experimental design for formulating FRT X<sub>1</sub>: Ac-Di-Sol, X<sub>2</sub>: Sodium starch glycolate

Batches	Variable Levels in Coded Form	
	X <sub>1</sub>	X <sub>2</sub>
F1	-1	-1
F2	-1	0
F3	-1	+1
F4	0	-1
F5	0	0
F6	0	+1
F7	+1	-1
F8	+1	0
F9	+1	+1

**Table 3:** Actual values of coded variables for formulating FRT X1: Ac-Di-Sol, X2: Sodium starch glycolate

Coded values	Actual values (% w/w)	
	X <sub>1</sub> (% w/w)	X <sub>2</sub> (% w/w)
-1	2	2
0	4	4
+1	6	6

### Method of preparation of FRT

The direct compression technique was used for tablet preparation. All the raw materials were passed through a#60 (0.250 mm) sieve before mixing (Table 4). Terbutaline sulphate, sodium starch glycolate, Ac-Di-Sol, lactose and Avicel PH-101 were blended using a laboratory mortar and pestle. The powder blend was lubricated with 2% talc

**Table 4:** Composition of Terbutaline sulphate fast-release tablet formulations (Batches F1-F9 in mg)

Ingredients (mg)	F1	F2	F3	F4	F5	F6	F7	F8	F9
Terbutaline Sulphate	2	2	2	2	2	2	2	2	2
Ac-di-sol	2	2	2	2	2	2	2	2	2
Sodium starch glycolate	2	4	6	2	4	6	2	4	6
Avicel PH-101	30	30	30	30	30	30	30	30	30
Lactose	60	58	56	58	56	54	56	54	52

Magnesium Stearate	2	2	2	2	2	2	2	2	2
Talc	2	2	2	2	2	2	2	2	2

and 2% magnesium stearate. The powder blend was compressed on a single punch tablet machine.

### Response surface and statistical analysis of model

2-D contour plots and 3-D response surface plots were plotted to study the effect of independent variables on dependent variables. ANOVA and Lack-of-fit test analysis were done for the model to identify insignificant factors.

### Optimization of FRT

By using the quadratic equation obtained from factorial design optimized tablets were manufactured with DT targeted to 30 s and friability in a range between 0.42%-0.96% (Table 5).

**Table 5:** Optimization of FRT

Constraints			
	Goal	Lower limit	Upper limit
Na Response surface and statistical analysis of model 2-D contour plots and 3-D response surface plots were plotted to study the effect of independent variables on dependent variables. ANOVA and Lack-of-fit test analysis were done for the model to identify insignificant factors. Optimization of FRT By using the quadratic equation obtained from factorial design optimized tablets were manufactured with DT targeted to 30 s and friability in a range between 0.42%-0.96%			
X <sub>1</sub> -Acdisol	is in range	-1	+1
X <sub>2</sub> -SSG	is in range	-1	+1
DT (s)	is target=30	23	88
Friability (%)	is in range	0.42	0.96

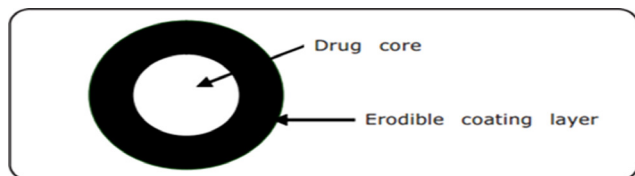
### Evaluation of optimized batch of FRT

For verifying, the model for its ability to predict 3 batches of the optimized batch were prepared, and evaluation was done.

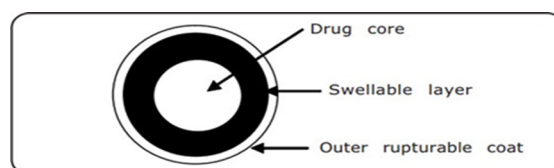
## Results and Discussion

### Drug analysis

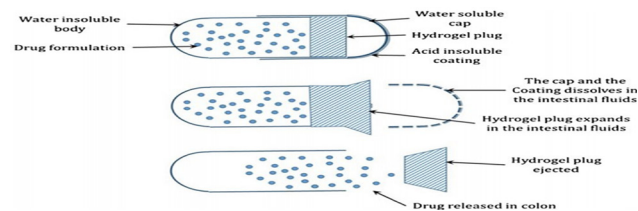
Drug (Terbutaline sulphate) sample was analysed using various physical, physicochemical and spectrophotometric methods. The sample was a white powder which was confirmed by the literature. From the analysis of the drug using various physical and spectrophotometric methods it was inferred that the obtained drug sample was pure as shown in Figures 1-4.



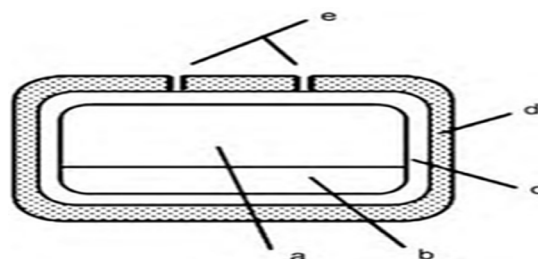
**Figure 1:** Diagram of the delivery system having erodible coatings



**Figure 2:** Outline of the delivery system with rupturable coating layers



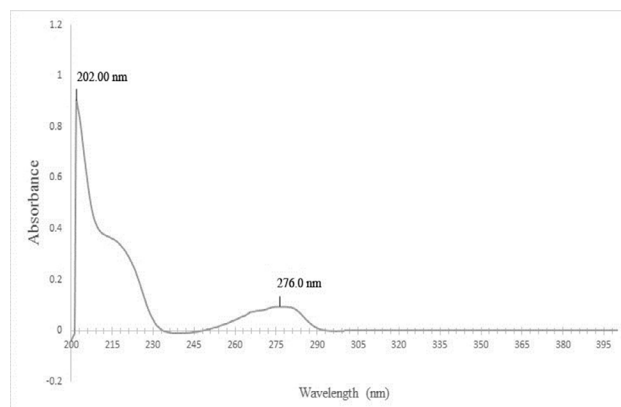
**Figure 3:** Outline of the mechanism of the release-controlling plug based drug delivery system



**Figure 4:** Outline of osmotic drug delivery system: (a) Drug formulation, (b) swelling polymeric compartment, (c) hydrophilic polymeric coating, (d) osmotic membrane and (e) laser-drilled orifices

### Melting point of the drug

The melting point is given in Table 6 the  $\lambda_{\max}$  were found to be 202 nm and 276 nm which matches the values given in literature. UV absorption spectra are shown in Figure 5.



**Figure 5:** UV absorption spectra of Terbutaline sulphate in buffer pH 1.2

**Table 6:** Melting point analysis data

Method used	Experimental value	Literature value <sup>100</sup>
Capillary fusion method	246°C-249°C	246°C-248°C

### FTIR spectra of the drug

FTIR spectroscopy was used to verify the authenticity of the sample and from the obtained spectra it was inferred

that characteristic peaks obtained (3300  $\text{cm}^{-1}$ -OH stretch, 3050  $\text{cm}^{-1}$ -aromatic CH stretch, 1200  $\text{cm}^{-1}$  phenolic C-O stretch, 1610  $\text{cm}^{-1}$ -aromatic ring stretch) were concordant with literature (Figure 6).

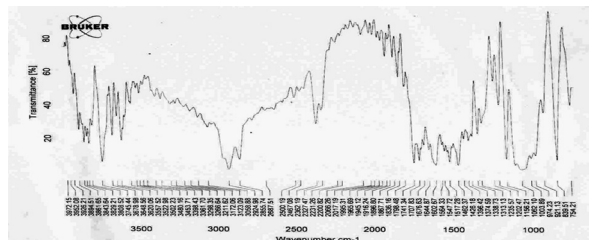


Figure 6: FTIR Spectra of Terbutaline sulphate Calibration curve

### Calibration curve

Calibration curves were prepared in a concentration range of 2  $\mu\text{g/mL}$ -20  $\mu\text{g/mL}$  and straight lines were obtained as shown in Figures 7 and 8. The equations of straight lines were found to be  $y=0.0085x-0.0005$  and  $y=0.0085x-0.001$  for buffer pH 1.2 and 6.8 respectively (Tables 7 and 8).

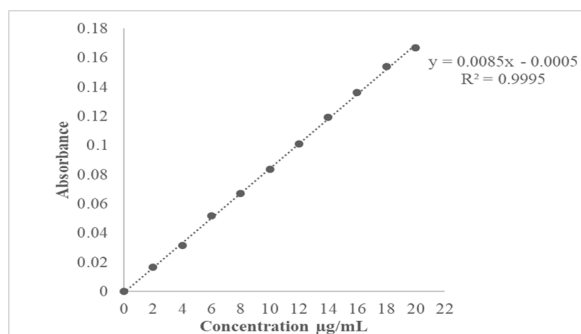


Figure 7: Calibration Curve of Terbutaline sulphate in Hydrochloric acid buffer pH 1.2

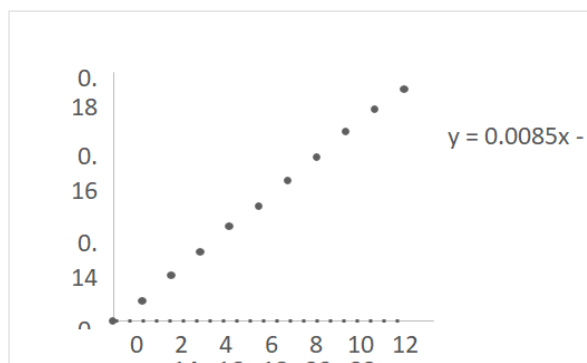


Figure 8: Calibration Curve of Terbutaline sulphate in phosphate buffer pH 6.8

Table 7: Calibration data of Terbutaline sulphate in Hydrochloric acid buffer pH 1.2 and phosphate buffer pH 6.8

S. No.	Concentration( $\mu\text{g/mL}$ )	Absorbance in pH 1.2	Absorbance in pH 6.8
1	2	0.0168	0.0143
2	4	0.0314	0.0331
3	6	0.0517	0.0502
4	8	0.0672	0.0683
5	10	0.0838	0.0832
6	12	0.1013	0.1016
7	14	0.1193	0.1189

8	16	0.1363	0.1373
9	18	0.154	0.1534
10	20	0.1671	0.1679

Table 8: Statistical Parameters related to calibration curve in Hydrochloric acid buffer pH 1.2 and phosphate buffer pH 6.8

S. No	Parameters	Value in pH 1.2	Value in pH 6.8
1	Equation of straight line	$y=0.0085x-0.0005$	$y=0.0085x-0.001$
2	Regression Coefficient	0.9995	$R^2=0.9996$

### Solubility study

Drug was freely soluble in water and had a solubility of 212.3 mg/ml (Table 9).

Table 9: Quantitative Solubility of Terbutaline sulphate in water at Room Temperature

S. No	Media	Solubility (mg/mL)
1	Distilled Water	212.3 $\pm$ 2.614

### Partition coefficient

The partition coefficient of the drug was found to be 0.87 which was similar to value given in literature (Table 10).

Table 10: Partition coefficient of Terbutaline sulphate

S. No	Method	Experimental	Literature value <sup>99,100</sup>
1	n-octanol partition coefficient	0.87 $\pm$ 0.058	0.9

### Drug polymer interaction studies

The drug polymer compatibility studies showed that drug is compatible with all the polymers and therefore drug and polymers can be used to make formulations.

### FTIR analysis for drug polymer interaction studies

The FTIR studies of physical mixture of the drug with different polymers showed no sign of interaction as the spectra of mixtures showed the peaks similar to the pure drug spectra (Figures 9-13).

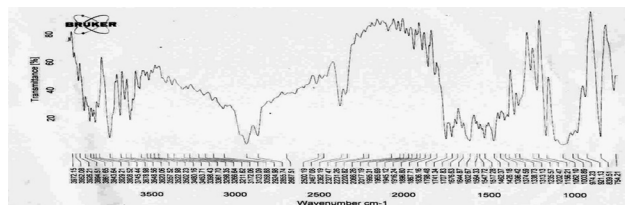


Figure 9: FTIR Spectra of Terbutaline sulphate

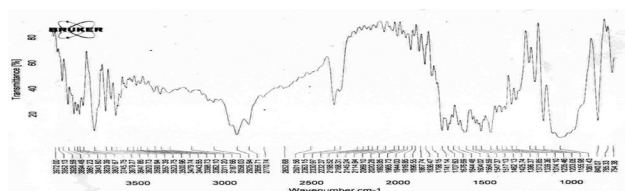
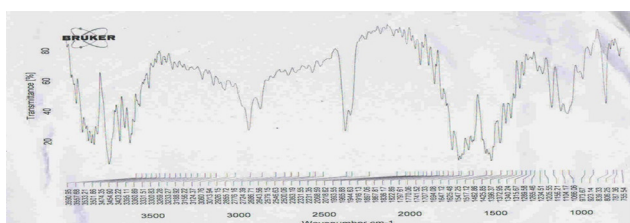
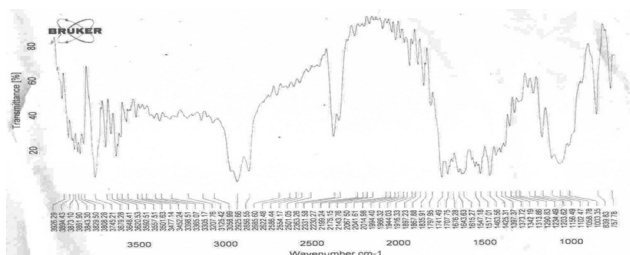


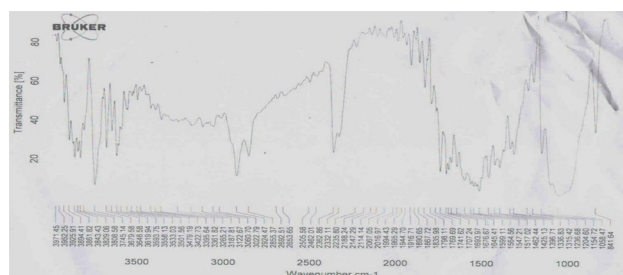
Figure 10: FTIR Spectra of physical mixture of Terbutaline sulphate and HPMC K15M



**Figure 11:** FTIR Spectra of physical mixture of Terbutaline sulphate and Carbolpol 971P



**Figure 12:** FTIR Spectra of physical mixture of Terbutaline sulphate and Ethyl cellulose



**Figure 13:** FTIR Spectra of physical mixture of Terbutaline sulphate and Ac-Di-Sol

### Preliminary studies for formulating FRT of Terbutaline sulphate

A total of 16 Preliminary trial batches were manufactured to check the result of concentration of super disintegrants on various physical properties of the manufactured tablets. In batches TF1-6 the concentration of Ac-Di-Sol was varied from 1-6%w/w while in batches TF7-12 concentration of sodium starch glycolate was varied from 1% w/w-6%w/w. Batches TF13-16 were combination batches having both the super disintegrants (Table 11).

**Table 11:** Characterization of FRT powder blend batches (TF1-15). Results are average of three determinations (Mean  $\pm$  SD)

Batches	BD (gm/cc)	TD (gm/cc)	CI (%)	HR	AOR ( $^{\circ}$ )
TF1	0.431 $\pm$ 0.032	0.481 $\pm$ 0.016	10.395 $\pm$ 1.23	1.116 $\pm$ 0.045	22.02 $\pm$ 0.218
TF2	0.425 $\pm$ 0.025	0.476 $\pm$ 0.028	10.714 $\pm$ 2.45	1.120 $\pm$ 0.037	23.91 $\pm$ 0.341
TF3	0.419 $\pm$ 0.022	0.473 $\pm$ 0.018	11.416 $\pm$ 3.56	1.128 $\pm$ 0.014	23.71 $\pm$ 0.242
TF4	0.413 $\pm$ 0.037	0.471 $\pm$ 0.031	12.314 $\pm$ 2.31	1.140 $\pm$ 0.034	22.63 $\pm$ 0.561
TF5	0.408 $\pm$ 0.012	0.468 $\pm$ 0.036	12.820 $\pm$ 3.67	1.147 $\pm$ 0.026	24.35 $\pm$ 0.378
TF6	0.402 $\pm$ 0.038	0.462 $\pm$ 0.024	12.987 $\pm$ 1.22	1.149 $\pm$ 0.017	22.27 $\pm$ 0.217
TF7	0.433 $\pm$ 0.025	0.483 $\pm$ 0.021	10.351 $\pm$ 2.89	1.115 $\pm$ 0.032	22.56 $\pm$ 0.341
TF8	0.426 $\pm$ 0.025	0.478 $\pm$ 0.037	10.878 $\pm$ 1.47	1.122 $\pm$ 0.024	23.3 $\pm$ 0.165
TF9	0.421 $\pm$ 0.015	0.477 $\pm$ 0.016	11.740 $\pm$ 4.26	1.130 $\pm$ 0.016	22.4 $\pm$ 0.349
TF10	0.416 $\pm$ 0.034	0.474 $\pm$ 0.023	12.236 $\pm$ 3.37	1.139 $\pm$ 0.034	24.71 $\pm$ 0.521
TF11	0.414 $\pm$ 0.031	0.471 $\pm$ 0.027	12.101 $\pm$ 1.26	1.137 $\pm$ 0.015	22.48 $\pm$ 0.382
TF12	0.411 $\pm$ 0.036	0.469 $\pm$ 0.032	12.366 $\pm$ 2.78	1.141 $\pm$ 0.023	22.71 $\pm$ 0.285
TF13	0.436 $\pm$ 0.022	0.487 $\pm$ 0.019	10.472 $\pm$ 2.27	1.169 $\pm$ 0.031	24.26 $\pm$ 0.378
TF14	0.418 $\pm$ 0.039	0.478 $\pm$ 0.052	12.552 $\pm$ 1.36	1.143 $\pm$ 0.024	25.31 $\pm$ 0.216
TF15	0.410 $\pm$ 0.036	0.462 $\pm$ 0.049	11.412 $\pm$ 3.21	1.122 $\pm$ 0.012	26.43 $\pm$ 0.218
TF16	0.411 $\pm$ 0.042	0.464 $\pm$ 0.041	11.422 $\pm$ 3.45	1.128 $\pm$ 0.018	26.72 $\pm$ 0.290

### Pre-compression characterization of FRT powder blends

Tablets were tested for pre-compression studies and the results revealed that all the batches possessed good flow properties. The bulk and TD of the batches (TF1-16) were within range of 0.402 gm/cc-0.436 gm/cc and 0.461 gm/cc-0.487 gm/cc respectively. By using the values of bulk and tapped densities, CI and HR were calculated. If the powder blend is more compressible then the powder will be less flowable and vice versa. The value of CI and HR was found to be within range between 10.351%-12.987% and 1.116-1.169 respectively. As the value of HR was less than 1.25, the shows good flow properties. The AOR below 30 $^{\circ}$  range indicates well to excellent flow properties of powder. Lower the friction occurring within the mass, better the flow rate. The AOR was found to be in range 22.02 $^{\circ}$ -26.72 $^{\circ}$ .

### Post-compression characterization of FRT

After compression of the powder blends, the tablets were tested for the post-compression characteristics such as appearance, thickness, hardness, drug content friability and disintegration time. The thickness varied from 2.18 mm-2.50 mm and weight varied between 99.46 mg-101.16 mg. The thickness and weight of tablets were under passable limits. Hardness was in range between 2.78 kg/cm $^2$ -3.63 kg/cm $^2$ . Only batch TF16 was outside passable limit with a hardness value of 2.78 kg/cm $^2$   $\pm$  0.234 0 kg/cm $^2$ . Drug content were in range between 99.82%-102.31% which is under passable limits. The friability of the tablets varied between 0.30%-1.72%. A value of friability less than 1% shows transport stress withstanding properties and batches TF1-15 passed this test while batch TF16 showed a value of 1.72%  $\pm$  0.048% which was outside passable limit. From the evaluation of preliminary trial batches, it can

be summed that concentration of each disintegrants had a negative effect on disintegration time. The disintegration time decreased from 122.24 s to 18.82 s as the concentration of Ac-Di-Sol was increased from 1%-6% w/w while the value of disintegration time decreased from 134.27 to 75.18 for sodium starch glycolate at same concentrations. The combination batches TF13-16 showed lesser values of disintegration time with TF16 showing disintegration time

value of 14.18 s which was least of all the batches. It can be inferred from evaluation parameters of the batch TF16 that when both the super disintegrants were used at concentration level of 9% w/w the manufactured tablets showed a lack of mechanical strength. Therefore, the level of super disintegrants for formulating factorial design batches was set at 2% w/w, 4% w/w and 6% w/w for the individual super disintegrant (Tables 12 and 13).

**Table 12:** Post-compression Characterization of FRT batches (TF1-TF16) (All values represent mean  $\pm$  standard deviation,  $\alpha$  n=3,  $\beta$  n=20,  $\gamma$  n=10)

Batches	Thickness $\alpha$ (mm)	Average Weight $\beta$ (mg)	Hardness $\alpha$ (kg/cm $^2$ )	Friability $\alpha$ (%)	Disintegration-Time $\alpha$ (s)	Drug content $\gamma$ (%w/w)
TF1	2.27 $\pm$ 0.18	100.36 $\pm$ 3.183	3.32 $\pm$ 0.125	0.60 $\pm$ 0.078	122.24 $\pm$ 2.46	100.43 $\pm$ 1.25
TF2	2.49 $\pm$ 0.015	100.72 $\pm$ 3.074	3.49 $\pm$ 0.241	0.37 $\pm$ 0.169	113.52 $\pm$ 2.92	100.66 $\pm$ 1.735
TF3	2.32 $\pm$ 0.215	101.58 $\pm$ 2.311	3.48 $\pm$ 0.237	0.35 $\pm$ 0.123	102.87 $\pm$ 1.27	99.82 $\pm$ 0.757
TF4	2.19 $\pm$ 0.087	101.00 $\pm$ 3.321	3.40 $\pm$ 0.118	0.48 $\pm$ 0.22	96.28 $\pm$ 2.38	100.79 $\pm$ 0.822
TF5	2.43 $\pm$ 0.131	99.55 $\pm$ 2.762	3.66 $\pm$ 0.095	0.61 $\pm$ 0.243	82.14 $\pm$ 3.55	101.02 $\pm$ 1.526
TF6	2.18 $\pm$ 0.029	101.05 $\pm$ 2.623	3.54 $\pm$ 0.103	0.43 $\pm$ 0.165	62.82 $\pm$ 3.37	100 $\pm$ 1.321
TF7	2.32 $\pm$ 0.122	100.4 $\pm$ 3.103	3.61 $\pm$ 0.195	0.51 $\pm$ 0.172	134.27 $\pm$ 3.45	100.22 $\pm$ 1.359
TF8	2.38 $\pm$ 0.188	101.04 $\pm$ 2.954	3.48 $\pm$ 0.249	0.56 $\pm$ 0.246	121.19 $\pm$ 2.9	100.59 $\pm$ 1.293
TF9	2.46 $\pm$ 0.131	99.97 $\pm$ 2.905	3.36 $\pm$ 0.086	0.67 $\pm$ 0.106	110.28 $\pm$ 3.32	100.01 $\pm$ 1.043
TF10	2.32 $\pm$ 0.237	99.46 $\pm$ 2.575	3.34 $\pm$ 0.182	0.51 $\pm$ 0.155	98.19 $\pm$ 1.76	100.13 $\pm$ 1.158
TF11	2.44 $\pm$ 0.15	101.16 $\pm$ 3.123	3.62 $\pm$ 0.162	0.50 $\pm$ 0.04	87.83 $\pm$ 3.11	100.59 $\pm$ 0.845
TF12	2.50 $\pm$ 0.026	100.02 $\pm$ 3.235	3.50 $\pm$ 0.187	0.58 $\pm$ 0.238	75.18 $\pm$ 2.51	100.48 $\pm$ 1.217
TF13	2.36 $\pm$ 0.18	100.21 $\pm$ 3.354	3.63 $\pm$ 0.144	0.63 $\pm$ 0.032	78.36 $\pm$ 4.33	99.45 $\pm$ 2.371
TF14	2.30 $\pm$ 0.123	100.67 $\pm$ 2.828	3.13 $\pm$ 0.135	0.74 $\pm$ 0.071	35.22 $\pm$ 2.56	102.31 $\pm$ 4.17
TF15	2.19 $\pm$ 0.11	99.97 $\pm$ 2.849	3.76 $\pm$ 0.216	0.41 $\pm$ 0.043	17.16 $\pm$ 3.21	100.33 $\pm$ 2.76
TF16	2.28 $\pm$ 0.206	99.95 $\pm$ 3.157	2.78 $\pm$ 0.234	1.72 $\pm$ 0.048	14.18 $\pm$ 3.82	100.67 $\pm$ 2.39

### Response surface analysis

2-D contour plots and 3-D response surface plots provide information about effect of independent variables on dependent variables. From the 2-D contour plot it can be seen that as the level of  $X_1$  and  $X_2$  were increased from -1 to 1, the disintegration time decreased from 77 s to 18 s (Figure 14). Response surface plot also depicts similar antagonistic effect of  $X_1$  and  $X_2$  on disintegration time (Figure 15). 2-D contour plot and response surface plot depict the synergistic effect of independent variables  $X_1$  (Figures 16 and 17). Plot shows that as the levels of  $X_1$  were increased from -1 to 1, the friability increased from 0.248% to 0.771% while as the levels of  $X_2$  were increased friability decreased. A linear behavior was seen between independent and dependent variables.

The quadratic equations for both the responses are shown below.

(For disintegration time)

$$Y_1 = +40.59 - 10.00X_1 - 18.67X_2 - 2.25X_1X_2 + 4.45X_1^2 + 3.45X_2^2$$

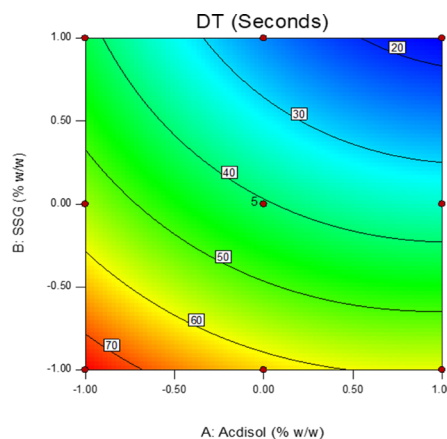
(For friability)

$$Y_2 = +0.60 + 0.070X_1 - 0.17X_2 + 0.020X_1X_2 + 0.023X_1^2 -$$

$$0.085X_2^2$$

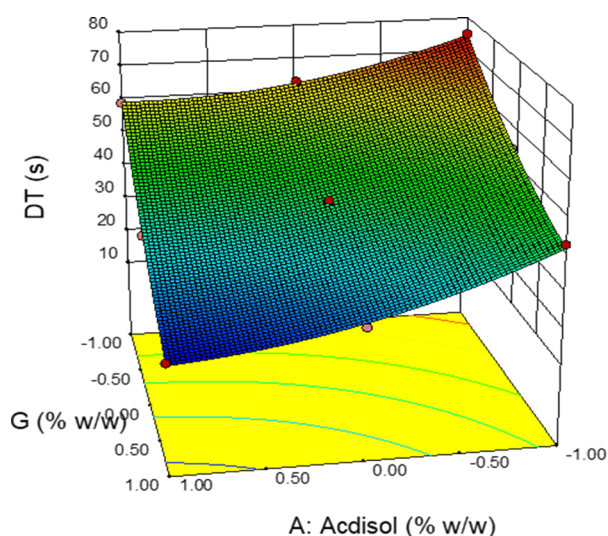
### Effect of formulation variables on friability

Friability was found to vary between 0.25% to 0.78%. Friability should be less than 1.0% and all the batches passed this criterion. As the coefficient  $b_1$  has a positive sign this means that increase in concentration of Ac-di-sol lead to an increased friability. At higher levels of Ac-di-sol mechanically weak tablets were produced. As the concentration of sodium starch glycolate was increased the disintegration time decreased.



**Figure 14:** 2-D contour plot displaying influence of independent variables  $X_1$  and  $X_2$  on dependent variable  $Y_1$  (Disintegration time)





**Figure 15:** 3-D response surface plot displaying influence of independent variables  $X_1$  and  $X_2$  on dependent variable  $Y_1$  (Disintegration time)

#### Effect of formulation variables on disintegration time

As the concentration of Ac-di-sol or sodium starch glycolate were increased the disintegration time decreased, Higher Ac-di-sol concentration lead to quick disintegration as the polymers swelled on absorbing water and caused disintegration of tablet due to the pressure generated. Higher concentration of sodium starch glycolate also decreased the disintegration time as this polymer absorbs moisture by wicking. Disintegration time is one of the most important criteria in developing FRT and the disintegration time varied between 18 s to 75 s.

**Table 14:** Analysis of variance and lack-of-fit tests for the response surface model  $Y_1$  (Disintegration time)

Source	Sum of Squares	df	Mean Square	F Value	p-value Prob > F	PRESS	R2 Value
Model	2851.02	5	570.2	261.04	<0.0001	-	-
$X_1$ -Acdisol	600	1	600	274.69	<0.0001	55.91	0.9947
$X_2^2$ -SSG	2090.67	1	2090.67	957.13	<0.0001	-	-
$X_1 X_2$	20.25	1	20.25	9.27	0.0187	-	-
$X_1$	54.65	1	54.65	25.02	0.0016	-	-
$X_2$	32.84	1	32.84	15.03	0.0061	-	-
Residual	15.29	7	2.18	-	-	-	-
Lack of Fit	4.49	3	1.5	0.55	0.6722	-	-
Pure Error	10.8	4	2.7	-	-	-	-
Cor. Total	2866.31	12	-	-	-	-	-

**Table 15:** Analysis of variance and lack-of-fit tests for the response surface model  $Y_2$  (Friability)

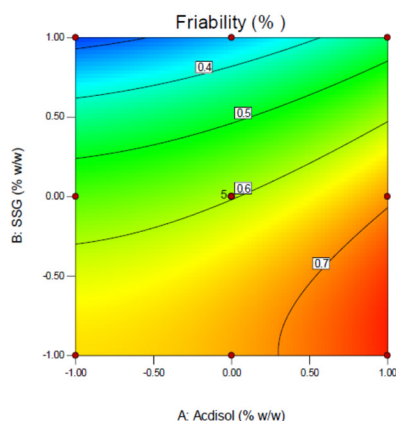
Source	Sum of Squares	df	Mean Square	F Value	p-value Prob > F	PRESS	R2 Value
Model	0.23	5	0.045	44.32	<0.0001	-	-
$X_1$ -Acdisol	0.029	1	0.029	28.62	0.0011	0.04	0.9694
$X_2^2$ -SSG	0.17	1	0.17	171.78	<0.0001	-	-
$X_1 X_2$	1.60E-03	1	1.60E-03	1.57	0.2501	-	-
$X_2$	1.52E-03	1	1.52E-03	1.5	0.2607	-	-
$X_2$	0.02	1	0.02	19.39	0.0031	-	-
Residual	7.12E-03	7	1.02E-03	-	-	-	-
Lack of fit	4.05E-03	3	1.350E-03	1.76	0.2936	-	-
Pure error	0.23	5	0.045	44.32	<0.0001	-	-
Cor. Total	0.029	1	0.029	28.62	0.0011	-	-

#### ANOVA and Lack-of-fit test

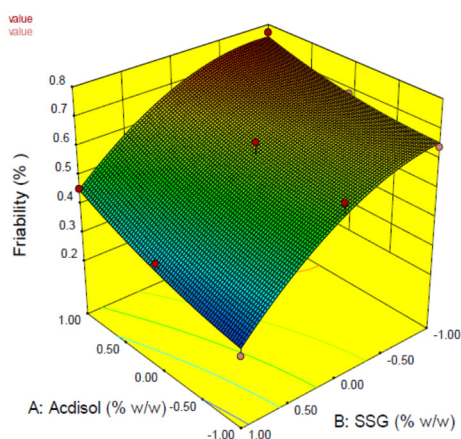
ANOVA and Lack-of-fit test analysis were done for the model (Tables 13-15). The results of the ANOVA, were applied to identify insignificant factors. The Model F-value of 261.04 and 44.32 with a p-value of <0.0001 were significant which implies that the models were significant. Values of "Probability>F" less than 0.0500 indicate model terms are significant. In this case  $X_1$ ,  $X_2$  are significant model terms. Predicted Residual Sum of Squares (PRESS) is a measure to determine the fittingness of each design point in the model. Value of PRESS was found to be 55.91 and 0.043 for both responses which were small, smaller the PRESS statistic, better the model fits the data points. High R square value of 0.9947 and 0.9694 for both responses suggested that these models are significant. Lack of fit is an unwanted characteristic for a model. A significant value of lack of fit test shows that the model does not fit the data well. In our case, the p-value for the lack of fit of the 2 models was 0.6722 and 0.2936 and both the values were insignificant, so the model fits the data generated. The model showed a statistically insignificant lack of fit.

**Table 13:** Levels of superdisintegrants selected for experimental design batches for formulating FRT

Superdisintegrants	
Ac-Di-Sol (%w/w)	Sodium starch glycolate (%w/w)
2	2
4	4
6	6



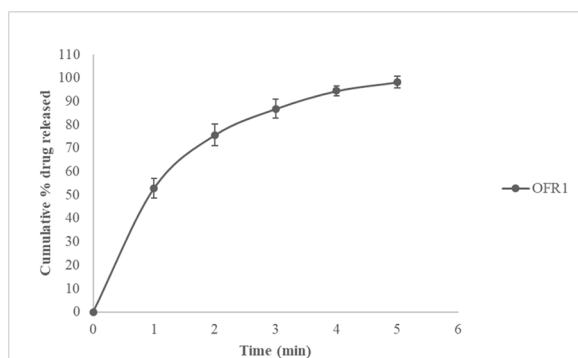
**Figure 16:** 2-D contour plot displaying effect of independent variables  $X_1$  and  $X_2$



**Figure 17:** 3-D Response surface plot displaying influence of independent variables  $X_1$  and  $X_2$  on dependent variable  $Y_2$  (Friability)

### Optimization and characterization of FRT

The suggested optimized formulation was 0.509 and 0.358 for  $X_1$ , and  $X_2$  respectively, with the corresponding desirability (D) value of 1.00. This factor level combination predicted the response as  $Y_1=30$  s and  $Y_2=0.570\%$  (Table 16). To confirm the model adequacy for the prediction, 3 batches of the optimized formulations (OFR1) were prepared and all the evaluation parameters were performed (Tables 17 and 18). *In vitro* release studies were also performed for optimized batch of FRT shown in Figure 18.



**Figure 18:** *In vitro* release profile of Terbutaline sulphate from optimized

batch of fast release formulations (OFR1)

**Table 16:** Model predicted levels of dependent and independent variables

Solution				
Ac-di-sol ( $X_1$ )	SSG ( $X_2$ )	DT (s)	Friability $\alpha$ (%)	Desirability
0.509	0.358	30	0.57	1

**Table 17:** Evaluation results of optimized batch of FRT (OFR1)

Hardness $\alpha$ (Kg/cm $^2$ )	Friability $\alpha$ (%)	Disintegration time $\alpha$ (s)	Drug Content (%w/w)	Average Weight $\beta$ (mg)
$3.19 \pm 0.06$	$0.58 \pm 0.021$	$31.67 \pm 0.577$	$100.56 \pm 1.79$	$101.35 \pm 1.95$

**Table 18:** *In Vitro* release profile data of cumulative % Terbutaline sulphate released from optimized batch of FRT

Time (min)	Cumulative % release
1	$52.49 \pm 4.252$
2	$75.95 \pm 4.565$
3	$88.02 \pm 2.485$
4	$94.36 \pm 1.923$
5	$98.93 \pm 0.849$

### Conclusion

Present research was aimed at developing chrono modulated drug delivery formulation for the treatment of nocturnal asthma. To determine the authenticity of the drug sample (Terbutaline sulphate), various physical, physicochemical and spectrophotometric methods were employed. UV and FTIR spectroscopy were used to verify the authenticity of the sample and the sample was found to be authentic. Drug polymer compatibility studies were conducted and no sign of physical compatibility was seen. The FTIR studies of physical mixture of the drug with different polymers showed no sign of interaction as the spectra of mixtures showed the peaks similar to pure drug spectra. UV spectroscopic method was selected as preferred analytical method for determination of Terbutaline sulphate. Trial batches (preliminary) were formulated to study influence of polymer concentration on the physical properties and release profiles of the formulations. The final concentration of the polymers to be used in experimental design was fixed using the preliminary trial batches data.

### Acknowledgement

None.

### Conflict of Interest

Authors have no conflict of interest to declare.

### References

1. B.G. Katzung, S.B. Masters, A.J. Trevor, Basic & clinical pharmacology bertram, J McGraw-Hill Education, 1(2003).
2. M.H. Smolensky, Chronobiology and chronotherapeutics applications to cardiovascular medicine, Am J Hematol, 9(1996):11-21.
3. A. Reinberg, M.H. Smolensky, Biologic rhythms

- and medicine, cellular, metabolic, pathophysiologic, and pharmacologic aspects, Springer Verlag GmbH, 305(1983).
4. E. Haus, Y. Touitou, *Biologic rhythms in clinical and laboratory medicine*, Springer-Verlag, Heidelberg, 730(1992).
  5. M.H. Smolensky, N.A. Peppas, *Chronobiology, drug delivery, and chronotherapeutics*, *Adv Drug Del Revs*, 59(2007):828–851.
  6. H. Dardente, N. Cermakian, Review: Molecular circadian rhythms in central and peripheral clocks in mammals, *J Chronobiol Int*, 24(2007):195–214.
  7. D. Duguay, N. Cermakian, The crosstalk between physiology and circadian clock proteins, *Chronobiol Int*, 26(2009):1479–1513.
  8. J.P. Hanifin, G.C. Brainard, Photoreception for circadian, neuroendocrine, and neurobehavioral regulation, *J Physiol Anthropol*, 26(2007):87–94.
  9. E. Maronde, J.H. Stehle, The mammalian pineal gland: Known facts, unknown facets, *Trends Endocrinol Metab*, 18(2007):142–149.
  10. D.A. Golombek, D.E. Rosenstein, Physiology of circadian entrainment, *Physiol Rev*, 90(2010):1063–1102.
  11. D. Duguay, N. Cermakian, The crosstalk between physiology and circadian clock proteins, *Chronobiol Int*, 26(2009):1479–1513.
  12. T. Bussemer, N.A. Peppas, R. Bodmeier, Evaluation of the swelling, hydration and rupturing properties of the swelling layer of a rupturable pulsatile drug delivery system, *Eur J Pharm Biopharm*, 56(2003):261–270.